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Determination of ambient concentrations of  
several analytes

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Field of the invention

The present invention relates to the determination of ambient analyte concentrations in liquids, for example the determination of analytes such as hormones, proteins and other naturally occurring or artificially present substances in biological liquids such as body fluids.

Background of the invention

10 I have proposed in International Patent Application WO84/01031 to measure the concentration of an analyte in a fluid by contacting the fluid with a trace amount of a binding agent such as an antibody specific for the analyte in the sense that it reversibly binds the analyte but not  
15 other components of the fluid, determining a quantity representative of the proportional occupancy of binding sites on the binding agent and estimating from that quantity the analyte concentration. In that application I point out that, provided that the amount of binding agent  
20 is sufficiently low that its introduction into the fluid causes no significant diminution of the concentration of ambient (unbound) analyte, the fractional occupancy of the binding sites on the binding agent by the analyte is effectively independent of the absolute volume of the fluid  
25 and of the absolute amount of binding agent, i.e. independent within the limits of error usually associated with the measurement of fractional occupancy. In such circumstances, and in these circumstances only, the initial concentration [H] of analyte in the fluid is related to the  
30 fraction  $(Ab/Ab_0)$  of binding sites on the binding agent occupied by the analyte by the equation:

$$\frac{Ab}{Ab_0} = \frac{K_{ab}[H]}{1 + K_{ab}[H]}$$

where  $K_{ab}$  (hereinafter referred to as  $K$ ) is the equilibrium constant for the binding of the analyte to the binding sites and is a constant for a given analyte and binding agent at any one temperature. This constant is generally known as the affinity constant, especially when the binding agent is an antibody, for example a monoclonal antibody.

The concept of using only a trace amount of binding agent is contrary to generally recommended practice in the field of immunoassay and immunometric techniques. For example, in such a well-known work as "Methods in Investigative and Diagnostic Endocrinology", ed. S.A. Berson and R.S. Yalow, 1973 at pages 111-116, it is proposed that in the performance of a competitive immunoassay maximum sensitivity of the assay is achieved if the proportion of the "tracer" analyte that is bound approximates to 50%. In order to achieve such a high degree of binding of the analyte the theory of Berson and Yalow, to this day generally accepted by other workers in the field, requires that the concentration of binding agent (or, strictly speaking, of binding sites, each molecule of binding agent conventionally having one or at most two binding sites) must be greater than or equal to the reciprocal of the equilibrium constant ( $K$ ) of the binding agent for the analyte, i.e.  $[Ab] \geq 1/K$ . For a sample of volume  $V$  the total amount of binding agent (or binding sites) must therefore be greater than or equal to  $V/K$ . A binding agent which is a monoclonal antibody may, for example, have an equilibrium constant ( $K$ ) which is of the order of  $10^{11}$  litres/mole for the specific antigen to which it binds. Thus, under the above generally accepted practice, a binding agent (or site) concentration of the order of  $10^{-11}$  mole/litre or more is required for binding agents of such an equilibrium constant and, with fluid sample volumes of

the order of 1 millilitre, the use of  $10^{-14}$  or more mole of binding agent (or site) is conventionally deemed necessary. Avogadro's number is about  $6 \times 10^{23}$  so that  $10^{-14}$  mole of binding site is equivalent to more than  $10^9$  molecules of binding agent even assuming that the binding agent possesses two binding sites per molecule. For specific binding agents of the very highest affinity  $K$  is less than  $10^{13}$  litres/mole so that conventional practice requires more than  $10^7$  molecules of binding agent, whereas binding agents with lower affinity of the order of  $10^8$  litres/mole necessitate the use of more than  $10^{12}$  molecules under conventional practice. In fact all immunoassay kits marketed commercially at the present time conform to these concepts and use an amount of binding site approximating to or, more frequently, considerably in excess of  $V/K$ ; indeed in certain types of kit relying on the use of labelled antibodies it is conventional to use as much binding agent as possible, binding proportions of analyte greatly exceeding 50%.

Because of the binding of substantial proportions, for example 50%, of the analyte in the liquid samples under test in such systems, the fractional occupancy of the binding sites of the binding agent is not independent of the volume of the fluid sample so that for accurate quantitative assays it is necessary to control accurately the volume of the sample, keeping it constant in all tests, whether of the sample of unknown concentration or of the standard samples of known concentration used to generate the dose response curve. Furthermore, such systems also require careful control of the amount of binding agent present in the standard and control incubation tubes. These limitations of present techniques are universally recognised and accepted.

UK Patent Application 2,099,578A discloses a device for immunoassays comprising a porous solid support to which antigens, or less frequently immunoglobulins, are bound at

a plurality of spaced apart locations, said device permitting a large number of qualitative or quantitative immunoassays to be performed on the same support, for example to establish an antibody profile of a sample of human blood serum. However, although the individual locations may be in the form of so-called microdots produced by supplying droplets of antigen-containing solutions or suspensions, the number of moles of antigen present at each location is apparently still envisaged as being enough to bind essentially all of the analyte (e.g. antibody) whose concentration is to be measured that is present in the liquid sample under test. This is apparent from the fact that the quantitative method used in that application (page 3, lines 21-28) involves calibration with known amounts of immunoglobulin being applied to the support; but this means that, in the samples being tested, essentially every molecule must be extracted from the sample in order for a true comparison to be made and hence that large amounts of antigen (i.e. the binding agent in this situation) are required in each microdot, greatly in excess of the total amount of analyte (i.e. antibody in this situation) present in the sample.

#### Summary of the invention

The present invention involves the realisation that the use of high quantities of binding agent is neither necessary for good sensitivity in immunoassays nor is it generally desirable. If, instead of being kept as large as possible, the amount of binding agent is reduced so that only an insignificant proportion of the analyte is reversibly bound to it, generally less than 10%, usually less than 5% and for optimum results only 1 or 2% or less, not only is it no longer necessary to use an accurately controlled, constant volume for all the liquid samples (standard solutions and unknown samples) in a given assay, but it is also possible to obtain reliable and sometimes even improved estimates of analyte concentration using much

less than  $V/K$  moles of binding agent binding sites, say not more than  $0.1 V/K$  and preferably less than  $0.01 V/K$ . For a binding agent having an equilibrium constant ( $K$ ) for the analyte of the order of  $10^{11}$  litres/mole and samples of approximately 1 ml size this is approximately equivalent to not more than  $10^8$ , preferably less than  $10^7$ , molecules of binding agent at each location in an individual array. If the value of  $K$  is  $10^{13}$  litres/mole the figures are  $10^6$  and  $10^5$  molecules respectively, and if  $K$  is of the order of  $10^8$  litres/mole they are  $10^{11}$  and  $10^{10}$  molecules respectively. Below  $10^2$  molecules of binding agent at a single location the accuracy of the measurement would become progressively less as the fractional occupancy of the binding agent sites by the analyte would be able to change only in discrete steps as individual sites become occupied or unoccupied, but in principle at least the use of as low as 10 molecules would be permissible if an estimate with an accuracy of 10% is acceptable. Practical considerations may give rise to a preference for more than  $10^4$  molecules.

I have found that, generally speaking, for antibodies having an affinity constant  $K$  litres/mole for an antigen, the relationship between the antibody concentration and the fractional occupancy of the binding sites at any particular antigen concentration and the relationship between the antibody concentration and the percentage of antigen bound to the binding sites at any particular antigen concentration follow the same curves provided that the antibody concentrations and the antigen concentrations are each expressed in terms of fractions or multiples of  $1/K$ . This is illustrated by the accompanying drawing which is a graph representing two sets of curves plotting these relationships. Each curve relates to the antibody concentration  $[Ab]$ , expressed in terms of  $1/K$ , plotted along the x-axis. For the set of curves which remain constant or decline with increasing  $[Ab]$ , the y-axis represents the fractional occupancy ( $F$ ) of binding sites on the antibody by the antigen; for the second set, the y-axis

represents the percentage (b%) of antigen bound to those binding sites. The individual curves in each set represent the relationships corresponding to four different antigen concentrations [An] expressed in terms of K, namely 10/K, 1.0/K, 0.1/K and 0.01/K. The curves show that as [Ab] falls F reaches an essentially constant level, the value of which is dependant on [An].

c It will be appreciated ~~therefore~~ that the abovementioned GB patent application 2,099,578A, which for quantitative estimation relies on large amounts of binding agent and essentially total sequestration of all analyte, fails to recognise the advance achieved by the present invention, which instead relies on a different analytical principle requiring measurement of the fractional occupancy of the binding agent and which thus requires only a very low proportion of the total analyte molecules present to be sequestered from the sample.

Following the recognition that the use of such small amounts of binding agent is permissible, it becomes feasible to place the binding agent required for a single concentration measurement on a very small area of a solid support and hence to place in juxtaposition to one another but at spatially separate points on a single solid support a wide variety of different binding agents specific for different analytes which are or may be present simultaneously in a liquid to be analysed. Simultaneous exposure of each of the separate points to the liquid to be analysed will cause each binding agent spot to take up the analyte for which it is specific to an extent (i.e. fractional binding site occupancy) representative of the analyte concentration in the liquid, provided only that the volume of solution and the analyte concentration therein are large enough that only an insignificant fraction (generally less than 10%, usually less than 5%) of the analyte is bound to the point. The fractional binding site occupancy for each binding agent can then be determined

using separate site-recognition reagents which recognise either the unfilled binding sites or filled binding sites of the different binding agents and which are labelled with markers enabling the concentration levels of the separate reagents bound to the different binding agents to be measured, for example fluorescent markers. Such measurements may be performed consecutively, for example using a laser which scans across the support, or simultaneously, for example using a photographic plate, depending on the nature of the labels. Other imaging devices such as a television camera can also be used where appropriate. Because the binding agents are spatially separate from one another it is possible to use only a small number of different marker labels or even the same marker label throughout and to scan each binding agent location separately to determine the presence and concentration of the label. By use of the invention considerably more than 3 analyses can be performed with a single exposure of the solid support with liquid to be analysed, for example 10, 20, 30, 50 or even up to 100 or several hundreds of analyses.

Overall, therefore, the present invention provides a method for determining the ambient concentrations of a plurality of analytes in a liquid sample of volume V litres, comprising:

loading a plurality of different binding agents, each being capable of reversibly binding an analyte which is or may be present in the liquid and is specific for that analyte as compared to the other components of the liquid sample, onto a support means at a plurality of spaced apart locations such that each location has not more than  $0.1 V/K$  moles of a single binding agent, where K litres/mole is the equilibrium constant of the binding agent for the analyte,

contacting the loaded support means with the liquid sample to be analysed such that each of the spaced apart locations is contacted in the same operation with the liquid sample, the amount of liquid used in the sample

being such that only an insignificant proportion of any analyte present in the liquid sample becomes bound to the binding agent specific for it, and

measuring a parameter representative of the fractional  
5 occupancy by the analytes of the binding agents at the spaced apart locations by a competitive or non-competitive assay technique using a site-recognition reagent for each binding agent capable of recognising either the unfilled  
10 binding sites or the filled binding sites on the binding agent, said site-recognition reagent being labelled with a marker enabling the amount of said reagent in the particular location to be measured.

The invention also provides a device for use in determining the ambient concentrations of a plurality of  
15 analytes in a liquid sample of volume  $V$  litres, comprising a solid support means having located thereon at a plurality of spaced apart locations a plurality of different binding agents, each binding agent being capable of reversibly binding an analyte which is or may be present in the liquid  
20 sample and is specific for that analyte as compared to the other components of the liquid sample, each location having not more than  $0.1 V/K$ , preferably less than  $0.01 V/K$ , moles of a single binding agent, where  $K$  litres/mole is the equilibrium constant of that binding agent for reaction  
25 with the analyte to which it is specific.

A kit for use in the method according to the invention comprises a device according to the invention, a plurality of standard samples containing known concentrations of the analytes whose concentrations in the liquid sample are to  
30 be measured and a set of labelled site-recognition reagents for reaction with filled or unfilled binding sites on the binding agents.

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Detailed description

The choice of a solid support is a matter to be left



to the user. Preferably the support is non-porous so that the binding agent is disposed on its surface, for example as a monolayer. Use of a porous support may cause the binding agent, depending on its molecular size, to be  
5 carried down into the pores of the support where its exposure to the analyte whose concentration is to be determined may likewise be affected by the geometry of the pores, so that a false reading may be obtained. Porous supports such as nitrocellulose paper dotted with spots of  
10 binding agent are therefore less preferred. Unlike the supports used in GB 2,099,578A, which seem to need to be porous because of the large number of molecules to be attached, the supports for use in the present invention use much smaller quantities and therefore need not be  
15 porous. The non-porous supports may, for example be of plastics material or glass, and any convenient rigid plastics material may be used. Polystyrene is a preferred plastics material, although other polyolefins or acrylic or vinyl polymers could likewise be used.

20 The support means may comprise microbeads, e.g. of such a plastics material, which can be coated with uniform layers of binding agent and retained in specified locations, e.g. hollows, on a support plate. Alternatively the material may be in the form of a sheet or plate which is  
25 spotted with an array of dots of binding agent. It can be advantageous for the configuration of the support means to be such that liquid samples of approximately the volume V litres are readily retained in contact with the plurality of spaced apart locations marked with the different binding  
30 agents. For example, the spaced apart locations may be arranged in a well in the support means, and a plurality of wells, each provided with the same group of different binding agents in spaced apart locations, can be linked together to form a microtitre plate for use with a  
35 plurality of samples.

When the support means is to be used in conjunction

with a measuring system involving light scanning, the material, e.g. plastics, for the support is desirably opaque to light, for example it may be filled with an opacifying material which may inter alia be white or black, such as carbon black, when the signals to be measured from the binding agent or the site-recognition reagent are light signals, as from fluorescent or luminescent markers. In general, reflective materials are preferred in this case to enhance light collection in the detecting instrument or photographic plate. The final choice of optimum material is governed by its ability to attach the binding agent to its surface, its absence of background signal emission and its possession of other properties tending to maximise the signal/noise ratio for the particular marker or markers attached to the binding agent situated on its surface. Very satisfactory results have been obtained in the Examples described below by the use of a white opaque polystyrene microtitre plate commercially available from Dynatech under the trade name White Microfluor microtitre wells.

The binding agents used may be binding agents of different specificity, that is to say agents which are specific to different analytes, or two or more of them may be binding agents of the same specificity but of different affinity, that is to say agents which are specific to the same analyte but have different equilibrium constants  $K$  for reaction with it. The latter alternative is particularly useful where the concentration of analyte to be assayed in the unknown sample can vary over considerable ranges, for example 2 or 3 orders of magnitude, as in the case of HCG measurement in urine of pregnant women, where it can vary from 0.1 to 100 or more IU/ml.

The binding agents used will preferably be antibodies, more preferably monoclonal antibodies. Monoclonal antibodies to a wide variety of ingredients of biological fluids are commercially available or may be made by known

techniques. The antibodies used may display conventional affinity constants, for example from  $10^8$  or  $10^9$  litres/mole upwards, e.g. of the order of  $10^{10}$  or  $10^{11}$  litres/mole, but high affinity antibodies with affinity constants of  $10^{12}$ -  
5  $10^{13}$  litres/mole can also be used. The invention can be used with such binding agents which are not themselves labelled. However, it is also possible and frequently desirable to use labelled binding agents so that the system binding agent/analyte/site-recognition reagent  
10 includes two different labels of the same type, e.g. fluorescent, chemiluminescent, enzyme or radioisotopic, one on the binding agent and one on the site-recognition reagent. The measuring operation then measures the ratio of the intensity of the two signals and thus eliminates the  
15 need to place the same amount of labelled binding agent on the support when measuring signals from standard samples for calibration purposes as when measuring signals from the unknown samples. Because the system depends solely on measurement of a ratio representative of binding site  
20 occupancy, there is also no need to measure the signal from the entire spot but scanning only a portion is sufficient. Each binding agent is preferably labelled with the same label but different labels can be used.

The binding agents may be applied to the support in  
25 any of the ways known or conventionally used for coating binding agents onto supports such as tubes, for example by contacting each spaced apart location on the support with a solution of the binding agent in the form of a small drop, e.g. 0.5 microlitre, on a  $1\text{ mm}^2$  spot, and allowing them to  
30 remain in contact for a period of time before washing the drops away. A roughly constant small fraction of the binding agent present in the drop becomes adsorbed onto the support as a result of this procedure. It is to be noted that the coating density of binding agent on the microspot  
35 does not need to be less than the coating density in conventional antibody-coated tubes; the reduction in the number of molecules on each spot may be achieved solely by

reduction of the size of the spot rather than the coating density. A high coating density is generally desirable to maximise signal/noise ratios. The sizes of the spots are advantageously less than  $10 \text{ mm}^2$ , preferably less than  $1 \text{ mm}^2$ . The separation is desirably, but not necessarily, 2 or 3 times the radius of the spot, or more. These suggested geometries can nevertheless be changed as required, being subject solely to the limitations on the number of binding agent molecules in each spot, the minimum volume of the sample to which the array of spots will be exposed and the means locally available for conveniently preparing an array of spots in the manner described.

Once the binding agents have been coated onto the support it is conventional practice to wash the support, in the case of antibodies as binding agents, with a solution containing albumen or other protein to saturate all remaining non-specific adsorption sites on the support and elsewhere. To confirm that the amount of binding agent in an individual spot will be less than the maximum amount ( $0.1 \text{ V/K}$ ) required to conform to the principle of the present invention, the amount of binding agent present on any individual site can be checked by labelling the binding agent with a detectable marker of known specific activity (i.e. known amount of marker per unit weight of binding agent) and measuring the amount of marker present. Thus, if the use of labelled binder is not desired on the solid support used in the method of the invention the binding agent can nevertheless be labelled in a trial experiment and identical conditions to those found in that trial to give rise to correct loadings of binding agent can be used to apply unlabelled binding agent to the supports to be actually used.

The minimum size of the liquid sample ( $V$  litres) is correlated with the number of mole of binding agent (less than  $0.1 \text{ V/K}$ ) so that only an insignificant proportion of the analyte present in the liquid sample becomes bound to

the binding agent. This proportion is as a general rule less than 10%, usually less than 5% and desirably 1 or 2% or less, depending on the accuracy desired for the assay (greater accuracy being obtained, other things being equal, when smaller proportions of analyte are bound) and the magnitude of other error-introducing factors present. Sample sizes of the order of one or a few ml or less, e.g. down to 100 microlitres or less, are often preferred, but circumstances may arise when larger volumes are more conveniently assayed, and the geometry may be adjusted accordingly. The sample may be used at its natural concentration level or if desired it may be diluted to a known extent.

The site-recognition reagents used in the method according to the invention may themselves be antibodies, e.g. monoclonal antibodies, and may be anti-idiotypic or anti-analyte antibodies, the latter recognising occupied sites. Alternatively, for example for analytes of small molecular size such as thyroxine (T4), unoccupied sites may be recognised using either the analyte itself, appropriately labelled, or the analyte covalently coupled to another molecule - e.g. a protein molecule - which is directly or indirectly labelled. The site-recognition reagents may be labelled directly or indirectly with conventional fluorescent labels such as fluorescein, rhodamine or Texas Red or materials usable in time-resolved pulsed fluorescence such as europium and other lanthanide chelates, in a conventional manner. Other labels such as chemiluminescent, enzyme or radioisotopic labels may be used if appropriate. Each site-recognition reagent is preferably labelled with the same label but different labels can be used in different reagents. The site-recognition reagents may be specific for a single one of the binding agent/analyte spots in each group of spots or in certain circumstances, as with glycoprotein hormones such as HCG and FSH which have a common binding site, they may be cross-reacting reagents able to react with occupied binding sites in more than one

of the spots.

In the assay technique the signals representative of the fractional occupancy of the binding agent in the test samples of unknown concentrations of the analytes can be calibrated by reference to dose response curves obtained from standard samples containing known concentrations of the same analytes. Such standard samples need not contain all the analytes together, provided that each of the analytes is present in some of the standard samples. Fractional occupancy may be measured by estimating occupied binding sites (as with an anti-analyte antibody) or unoccupied binding sites (as with an anti-idiotypic antibody), as one is the converse of the other. For greater accuracy it is desirable to measure the fraction which is closer to zero because a change in fractional occupancy of 0.01 is proportionately greater in this case, although for fractional occupancies in the range 25-75% either alternative is generally satisfactory.

In that embodiment of the present invention which relies on two fluorescent markers, the measurement of relative intensity of the signals from the two markers, one on the binding agent and the other on the site recognition reagent, may be carried out by a laser scanning confocal microscope such as a Bio-Rad Lasersharp MRC 500, available from Bio-Rad Laboratories Ltd., and having a dual channel detection system. This instrument relies on a laser beam to scan the dots or the like on the support to cause fluorescence of the markers and wavelength filters to distinguish and measure the amounts of fluorescence emitted. Time-resolved fluorescence methods may also be used. Interference (so-called crosstalk) between the two channels can be compensated for by standard corrections if it occurs or conventional efforts can be made to reduce it. Discrimination of the two fluorescent signals emitted by the dual-labelled spots is accomplished in the present form of this instrument, by filters capable of distinguishing

the characteristic wavelength of the two fluorescent emissions; however, fluorescent substances may be distinguished by other physical characteristics such as differing fluorescence decay times, bleaching times, etc., and any of these means may be used, either alone or in combination, to differentiate between two fluorophores and hence permit measurement of the ratio of two fluorescent labelled entities (binding agent and site-recognition reagent) present on an individual spot, using techniques well known in the fluorescence measurement field. When only one fluorescent label is present the same techniques may be used, provided that care is taken to scan the entire spot in each case and the spots contain essentially the same amount of binding agent from one assay to the next when the unknown and standard samples are used.

In the case of other labels, such as radioisotopic labels, chemiluminescent labels or enzyme labels, analogous means of distinguishing the individual signals from one or from each of a pair of such labels are also well known. For example two radioisotopes such as  $^{125}\text{I}$  and  $^{131}\text{I}$  may be readily distinguished on the basis of the differing energies of their respective radioactive emissions. Likewise it is possible to identify the products of two enzyme reactions, deriving from dual enzyme-labelled antibody couplets, these being e.g. of different colours, or two chemiluminescent reactions, e.g. of different chemiluminescent lifetime or wavelength of light emission, by techniques well known in the respective fields.

The invention may be used for the assaying of analytes present in biological fluids, for example human body fluids such as blood, serum, saliva or urine. They may be used for the assaying of a wide variety of hormones, proteins, enzymes or other analytes which are either present naturally in the liquid sample or may be present artificially such as drugs, poisons or the like.

For example, the invention may be used to provide a device for quantitatively assaying a variety of hormones relating to pregnancy and reproduction, such as FSH, LH, HCG, prolactin and steroid hormones (e.g. progesterone, estradiol, testosterone and androstene-dione), or hormones of the adrenal pituitary axis, such as cortisol, ACTH and aldosterone, or thyroid-related hormones, such as T4, T3, and TSH and their binding protein TBG, or viruses such as hepatitis, AIDS or herpes virus, or bacteria, such as staphylococci, streptococci, pneumococci, gonococci and enterococci, or tumour-related peptides such as AFP or CEA, or drugs such as those banned as illicit improvers of athletes' performance, or food contaminants. In each case the binding agents used will be specific for the analytes to be assayed (as compared with others in the sample) and may be monoclonal antibodies therefor.

Further details on the methodology are to be found in my International Patent Publication WO88/01058, the contents of which are incorporated herein by reference.

The invention is illustrated by the following Examples.

#### Example 1

An anti-TNF (tumour necrosis factor) antibody having an affinity constant for TNF at 25°C of about  $1 \times 10^9$  litres/mole is labelled with Texas Red. A solution of the antibody at a concentration of 80 micrograms/ml is formed and 0.5 microlitre aliquots of this solution are added in the form of droplets one to each well of a Dynatech Microfluor (opaque white) filled polystyrene microtitre plate having 12 wells.

An anti-HCG (human chorionic gonadotropin) antibody having an affinity constant for HCG at 25°C of about  $6 \times 10^8$  litres/mole is also labelled with Texas Red. A



solution of the antibody at a concentration of 80 micrograms/ml is formed and 0.5 microlitre aliquots of this solution are added in the form of droplets one to each well of the same Dynatech Microfluor microtitre plate.

5        After addition of the droplets the plate is left for a few hours in a humid atmosphere to prevent evaporation of the droplets. During this time some of the antibody molecules in the droplets become adsorbed onto the plate. Next, the wells are washed several times with a phosphate  
10       buffer and then they are filled with about 400 microlitres of a 1% albumen solution and left for several hours to saturate the residual binding sites in the wells. Thereafter they are washed again with phosphate buffer.

      The resulting plate has in each of its wells two spots  
15       each of area approximately  $1 \text{ mm}^2$ . Measurement of the amount of fluorescence shows that in each well one spot contains about  $5 \times 10^9$  molecules of anti-TNF antibody and the other contains about  $5 \times 10^9$  molecules of anti-HCG antibody. The wells are designed for use with liquid  
20       samples of volume 400 microlitres, so that  $0.1 \text{ V/K}$  is  $4 \times 10^{-14}$  moles (equivalent to  $2.4 \times 10^{10}$  molecules) for the anti-TNF antibody and  $7 \times 10^{-14}$  moles (equivalent to  $4 \times 10^{10}$  molecules) for the anti-HCG antibody.

#### Example 2

25        A microtitre plate prepared as described in Example 1 is used in an assay for an artificially produced solution containing TNF and HCG. A test sample of the solution, amounting to about 400 microlitres, is added to one of the wells and allowed to incubate for several hours. About 400  
30       microlitres of various standard solutions containing known concentrations (0.02, 0.2, 2 and 20 ng/ml) of TNF or HCG are added to other wells of the plate and also allowed to incubate for several hours. The wells are then washed several times with buffer solution.

As site-recognition reagents there are used for the TNF spots an anti-TNF antibody having an affinity constant for TNF at 25°C of about  $1 \times 10^{10}$  litres/mole and for the HCG spots an anti-HCG antibody having an affinity constant for HCG at 25°C of about  $1 \times 10^{11}$  litres/mole. Both antibodies are labelled with fluorescein (FITC). 400 microlitre aliquots of solutions of these labelled antibodies are added to the wells and allowed to stand for a few hours. The wells are then washed with buffer.

The resulting fluorescence ratio of each spot is quantified with a Bio-Rad Lasersharp MRC 500 confocal microscope. From the standard solutions dose response curves for TNF and HCG are built up, the figures for TNF being as follows:

15	TNF concentration ng/ml	FITC fluorescence	on TNF spot
		<hr/> Texas Red fluorescence	
20	0.02	1.1	
	0.2	4.6	
	2	7.9	
	20	42.5	

and those for HCG being as follows:

25	HCG concentration ng/ml	FITC fluorescence	on HCG spot
		<hr/> Texas Red fluorescence	
	0.02	1.8	
	0.2	7.2	
	2	16.0	
	20	28.2	

The artificially produced solution was found to give ratio readings of 5.9 on the TNF spot and 10.5 on the HCG spot, correlating well with the actual concentrations of

TNF (0.5 ng/ml) and HCG (0.5 ng/ml) obtained from the dose response curves.

### Example 3

Using similar procedures to those outlined in Example 1 a microtitre plate containing spots of labelled anti-T4 (thyroxine) antibody (affinity constant about  $1 \times 10^{11}$  litres/mole at 25°C), labelled anti-TSH (thyroid stimulating hormone) antibody (affinity constant about  $5 \times 10^9$  litres/mole at 25°C) and labelled anti-T3 (triiodothyronine) antibody (affinity constant about  $1 \times 10^{11}$  litres/mole at 25°C) in each of the individual wells is produced, the spots containing less than  $1 \times 10^{-12}$  V moles of anti-T4 antibody or less than  $2 \times 10^{-11}$  V moles of anti-TSH antibody or less than  $1 \times 10^{-12}$  V moles of anti-T3 antibody.

The developing antibody (site-recognition reagent) for the TSH assay is an anti-TSH antibody with an affinity constant for TSH of  $2 \times 10^{10}$  litres/mole at 25°C. This antibody is labelled with fluorescein (FITC). The site-recognition reagents for the T4 and T3 assays are T4 and T3 coupled to poly-lysine and labelled with FITC, and they recognise the unfilled sites on their respective first antibodies.

Using 400 microlitre aliquots of standard solutions containing various known amounts of T4, T3 and TSH, dose response curves are obtained by methods analogous to those in Example 2, correlating fluorescence ratios with T4, T3 and TSH concentrations. The plate is used to measure T4, T3 and TSH levels in serum from human patients with good correlation with the results obtained by other methods.

### Example 4

Using similar procedures to those outlined in Example

1 a microtitre plate containing spots of first labelled  
anti-HCG antibody (affinity constant about  $6 \times 10^8$   
litres/mole at  $25^\circ\text{C}$ ), second labelled anti-HCG antibody  
(affinity constant about  $1.3 \times 10^{11}$  litres/mole at  $25^\circ\text{C}$ )  
5 and labelled anti-FSH (follicle stimulating hormone)  
antibody (affinity constant about  $1.3 \times 10^8$  litres/mole at  
 $25^\circ\text{C}$ ) in each of the individual wells is produced, the  
spots each containing less than 0.1 V/K moles of the  
respective antibody. A cross-reacting (alpha subunit)  
10 monoclonal antibody 8D10 with an affinity constant of  $1 \times$   
 $10^{11}$  litres/mole is used as a common developing antibody  
for both the HCG and the FSH assays.

Using 400 microlitre aliquots of standard solutions  
containing various known concentrations of HCG and FSH,  
15 dose response curves are obtained by methods analogous to  
those in Example 2, correlating fluorescence ratios with  
HCG and FSH concentrations, the curve obtained with the  
higher affinity anti-HCG antibody giving more concentra-  
tion-sensitive results at the lower HCG concentrations  
20 whereas the curve from the lower affinity anti-HCG antibody  
is more concentration-sensitive at the higher HCG con-  
centrations. The plate is used to measure HCG and FSH  
concentrations in the urine of women in pregnancy testing,  
giving good correlations with results obtained by other  
25 means and achieving effective concentration measurements  
for HCG over a concentration range of two or three orders  
of magnitude by correct choice of the best HCG spot and  
dose response curve.

#### Production of labelled antibodies

30 The labelling of the antibodies with fluorescent  
labels can be carried out by a well known and standard  
technique, see Leslie Hudson and Frank C. Hay, "Practical  
Immunology", Blackwell Scientific Publications (1980),  
pages 11-13, for example as follows:

The monoclonal antibody anti-FSH 3G3, an FSH specific (beta subunit) antibody having an affinity constant (K) of  $1.3 \times 10^8$  litres per mole, was produced in the Middlesex Hospital Medical School, and was labelled with TRITC (rhodamine isothiocyanate) or Texas Red, giving a red fluorescence.

The monoclonal antibody anti-FSH 8D10, a cross-reacting (alpha subunit) antibody having an affinity constant (K) of  $1 \times 10^{11}$  litres per mole, was likewise produced in the Middlesex Hospital Medical School and was labelled with FITC (fluorescein isothiocyanate), giving a yellow-green fluorescence.

The general procedure used involved ascites fluid purification (ammonium sulphate precipitation and T-gel chromatography) followed by labelling, according to the following steps:

1.a. Ammonium sulphate purification

1. Add 4.1 ml saturated ammonium sulphate solution to 5 ml antibody preparation (culture supernatant or 1:5 diluted ascites fluid) under constant stirring (45% saturation).

2. Continue stirring for 30-90 min. Centrifuge at 2500 rpm for 30 min.

3. Discard the supernatant and dissolve the precipitate in PBS (final volume 5 ml.). Repeat Steps 1 and 2, OR

4. Add 3.6 ml saturated ammonium sulphate (40% saturation) under constant stirring. Repeat Step 2.

5. Discard the supernatant and dissolve the pellet in the desired buffer.

6. Dialyse overnight in cold against the same buffer (using fresh, boiled-in-d/w dialysis bag).

7. Determine the protein concentration either at  $A_{280}$  or by Lowry estimation.

1.b. T-gel Chromatography: (Buffer: 1M Tris-Cl, pH 7.6. Solid potassium sulphate)

1. Clear 2 ml of ascites fluid by centrifugation at 4000 rpm.
- 5      2. Add 1 M Tris-Cl solution to achieve final concentration of 0.1 M.
3. Add sufficient amount of solid potassium sulphate. Final concentration = 0.5 M.
4. Apply the ascite fluid to the T-gel column.
- 10      5. Wash the column with 0.1 M Tris-Cl buffer containing 0.5 M potassium sulphate, until protein profile (at  $A_{280}$ ) returns to zero.
6. Elute the absorbed protein using 0.1 M Tris-Cl buffer as the eluant.
- 15      7. Pool the fractions containing antibody activity and concentrate using Amicon 30 concentrater.
8. If HPHT purification is to be carried out, use HPHT chromatography Starting buffer during Step 7.
2. Labelling of Antibodies FITC/TRITC conjugation:
- 20      1. Dialyse the purified 1 g protein into 0.25 M Carbonate-bicarbonate buffer, pH 9.0 to a concentration of 20 mg/ml.
2. Add FITC/TRITC to achieve a 1:20 ratio with protein (i.e. 0.05 mg for every 1 mg of protein).
- 25      3. Mix and incubate at 4°C for 16-18 hrs.
4. Separate the conjugated protein from unconjugated by:
- a. Sephadex G-25 chromatography for FITC label,
- or b. DEAE-Sephacel chromatography for TRITC/FITC label.
- 30      Buffer system:

PBS for (a).

0.005 M Phosphate, pH 8.0 and 0.18 M

Phosphate, pH 8.0 for (b).

Calculation of FITC: Protein coupling ratio:-

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$2.87 \times 0.D.495 \text{ nm}$

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$0.D.280 \text{ nm} - 0.35 \times 0.D.495 \text{ nm}$

Tox3ox